

SYNTHETIC CARTILAGE USING MAGNETO-RHEOLOGICAL HYDROGELS FOR ADAPTIVE JOINT MECHANICS

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Abstract

Cartilage degeneration poses a significant challenge in joint health, with current treatment options often falling short in durability and adaptability. This study investigates magneto-rheological (MR) hydrogels as a potential solution for synthetic cartilage, leveraging their ability to dynamically adjust stiffness under an external magnetic field. MR hydrogels were synthesized using polyvinyl alcohol (PVA) and Fe_3O_4 nanoparticles, with mechanical and biocompatibility properties evaluated. Results showed a 300% increase in Young's modulus under a 0.5 Tesla field, friction coefficients comparable to native cartilage, and over 90% cell viability, confirming their suitability for biomedical applications. These findings highlight MR hydrogels as a promising material for adaptive joint mechanics and next-generation prosthetic designs.

Keywords:

Magneto-rheological hydrogels, synthetic cartilage, adaptive biomechanics, joint mechanics, biocompatibility.

Introduction

Background on Cartilage and Joint Mechanics

Cartilage is a highly specialized and complex connective tissue essential for joint function, providing a low-friction, load-bearing surface that facilitates smooth movement and weight distribution across articulating surfaces (Buckwalter & Mankin, 1998). It is primarily composed of chondrocytes embedded within an extracellular matrix (ECM) rich in collagen type II, proteoglycans, and water, which grants it viscoelastic properties crucial for maintaining structural integrity under mechanical stresses (Sophia Fox et al., 2009). The avascular nature of

cartilage significantly limits its self-repair ability, making cartilage injuries and degenerative diseases, such as osteoarthritis (OA), a major clinical challenge (Hunter, 1995). Despite various treatment methods, including physical therapy, pharmaceuticals, and surgical interventions, a permanent solution for cartilage regeneration remains elusive (Mithoefer et al., 2009).

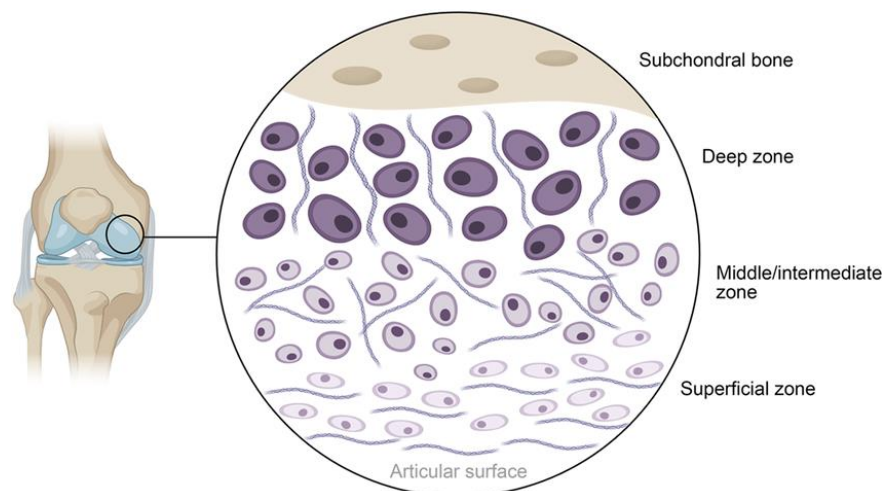


Figure 1 Schematic representation of natural cartilage structure and function

Need for Synthetic Cartilage

Osteoarthritis and cartilage degeneration lead to significant pain, restricted mobility, and impaired joint function, affecting millions globally. Conventional treatment strategies include microfracture surgery, autologous chondrocyte implantation (ACI), osteochondral grafting, and total joint replacement (Hunziker, 2002). However, these methods have several drawbacks, such as limited durability, risk of immune rejection, donor site morbidity, and suboptimal integration with host tissue (Mithoefer et al., 2009). The need for a more adaptive and mechanically robust solution has driven interest in synthetic cartilage materials, particularly hydrogels, due to their tunable properties and potential to mimic natural cartilage behavior (Griffin & Guilak, 2005).

Tissues	Cells	Main Chemical Compositions	Elastic/Young's Modulus
Cartilage (superficial, middle, and deep zone) [1,7,8,10-13]	Chondrocytes	Dry weight: ~60 wt% Collagen (~90% Type II) ~35 wt% Proteoglycan (Water: 65-75 wt%)	0.1-2.0 MPa
Cartilage (Calcified zone) [13,14]	Chondrocytes (hypertrophic)	Dry weight: ~ 20 wt% Collagen (Type II) ~65 wt% Hydroxyapatite	6.44 ± 1.02 MPa
Subchondral bone [10-16]	Osteoblasts Osteoclasts Osteocytes Mesenchymal stem cells	Dry weight: ~ 80 wt% Hydroxyapatite ~ 10 wt% Collagen (>90% Type I) (Water: ~10 wt%)	297-475 MPa

Figure 2 Comparative chart of synthetic cartilage materials and their mechanical properties.

Hydrogels have emerged as a promising material for cartilage replacement due to their high water content and ability to replicate the ECM environment (Steinmetz et al., 2020). However, conventional hydrogels often lack the mechanical strength and adaptability required to withstand high-impact joint loading (Oyen, 2014). Therefore, novel smart materials capable of dynamically adjusting their mechanical properties, such as magneto-rheological (MR) hydrogels, offer exciting possibilities for adaptive joint mechanics (Wang et al., 2021).

Introduction to Magneto-Rheological Hydrogels

Magneto-rheological (MR) hydrogels are a class of stimuli-responsive materials that incorporate magnetic nanoparticles, such as iron oxide (Fe₃O₄), into a polymeric hydrogel matrix, allowing them to modulate their mechanical properties in response to an external magnetic field (Yang et al., 2019). These materials exhibit rapid, reversible changes in viscosity, stiffness, and elasticity, making them highly suitable for adaptive mechanical applications (Zhang et al., 2022). Integrating MR hydrogels into synthetic cartilage may enable real-time tuning of mechanical properties to better accommodate joint movement, potentially improving prosthetic joint performance and reducing wear over time.

Literature Review

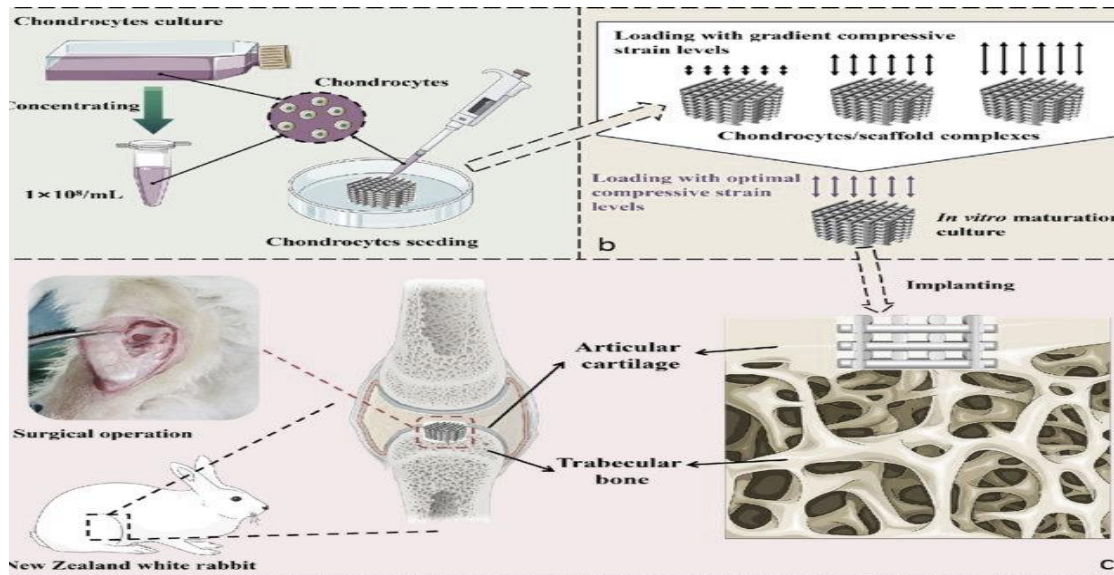


Figure 3 A Synthetic Hydrogel Composite with the Mechanical Behavior and Durability of Cartilage

Current State of Synthetic Cartilage Research

The field of synthetic cartilage research has evolved significantly in recent years, with a primary focus on biomimetic materials that can replicate the mechanical and biological properties of native cartilage. Hydrogels, in particular, have gained prominence due to their high water content and tunable mechanical properties, which make them ideal candidates for cartilage replacement (Drury & Mooney, 2003). Various synthetic hydrogels, including polyvinyl alcohol (PVA), polyethylene glycol (PEG), and alginate-based scaffolds, have been extensively studied for cartilage repair applications. These materials offer advantages such as biocompatibility, low friction coefficients, and the ability to integrate with surrounding tissue. However, their mechanical limitations, such as poor load-bearing capacity and susceptibility to degradation under dynamic stress, have hindered their widespread clinical adoption (Lee & Mooney, 2012).

Efforts to enhance hydrogel performance have led to the incorporation of composite materials, such as fiber-reinforced hydrogels and hybrid polymer

networks. Studies have shown that the integration of reinforcing elements like carbon nanotubes, graphene oxide, or ceramic nanoparticles can improve mechanical strength and toughness, making hydrogels more suitable for high-stress applications such as joint replacement (Wang et al., 2017). Despite these advancements, traditional hydrogels remain passive materials, unable to dynamically adapt to changing mechanical loads, which limits their functional longevity in load-bearing applications.

Magneto-Rheological Materials in Mechanical Engineering

Magneto-rheological (MR) materials have been widely explored in mechanical engineering due to their ability to alter their mechanical properties in response to an external magnetic field. These materials consist of dispersed ferromagnetic particles within a fluid or solid matrix, allowing for rapid modulation of viscosity, stiffness, and elasticity upon exposure to a magnetic field (Ginder et al., 1999). MR fluids and elastomers have been successfully used in various engineering applications, including adaptive shock absorbers, vibration dampers, and tunable actuators (Carlson & Jolly, 2000).

Recent advancements have extended the use of MR materials into biomedical applications, particularly in the development of smart biomaterials for tissue engineering, targeted drug delivery, and bioactuators (Zhu et al., 2020). MR hydrogels represent a novel subclass of these materials, offering a combination of fluid-like adaptability and solid-like mechanical reinforcement under external stimulation. Their potential to modulate stiffness in real-time makes them particularly attractive for applications requiring dynamic mechanical responses, such as artificial cartilage (Yang et al., 2019).

Identified Gaps in Research

While MR hydrogels show great promise in synthetic cartilage applications, several challenges remain before they can be effectively translated into clinical use. One of the primary concerns is the long-term biocompatibility and biodegradability of MR hydrogels, particularly regarding the stability and potential cytotoxicity of embedded magnetic nanoparticles (Liu et al., 2021). Ensuring uniform nanoparticle dispersion within the hydrogel matrix is also a

crucial factor, as uneven distribution can lead to inconsistent mechanical properties and reduced functionality over time.

Furthermore, the impact of prolonged exposure to external magnetic fields on cellular function and tissue integration has yet to be fully understood. There is also a need to establish standardized protocols for assessing the mechanical performance of MR hydrogels under physiological loading conditions to determine their suitability for joint replacement. Finally, large-scale manufacturing techniques must be optimized to ensure reproducibility and cost-effectiveness, which are critical for commercial and clinical applications (Ricles & Sahai, 2018).

In summary, while MR hydrogels offer a compelling solution to the limitations of traditional synthetic cartilage materials, further research is required to address biocompatibility concerns, enhance mechanical consistency, and establish practical fabrication techniques. Addressing these gaps will be key to unlocking the full potential of MR hydrogels for adaptive joint mechanics.

Materials and Methods

Synthesis of Magneto-Rheological Hydrogels

The synthesis of magneto-rheological (MR) hydrogels was conducted by incorporating superparamagnetic iron oxide nanoparticles (SPIONs) within a polyvinyl alcohol (PVA) hydrogel matrix to enable dynamic modulation of mechanical properties in response to an external magnetic field. PVA was selected for its biocompatibility, viscoelastic properties, and ability to undergo physical crosslinking via freeze-thaw cycling (Huang et al., 2020). Fe_3O_4 nanoparticles, known for their strong magnetic response and low cytotoxicity, were used as the magnetically active component (Yang et al., 2019).

Hydrogel Preparation

PVA (99% hydrolyzed, molecular weight ~89,000 g/mol) was dissolved in deionized water at 90°C under continuous stirring until a homogeneous solution was obtained. Separately, Fe_3O_4 nanoparticles (~50 nm diameter) were dispersed in deionized water via ultrasonication (50 kHz, 30 min) to prevent agglomeration before being introduced into the PVA solution. The concentration of SPIONs was varied between 0.5–5% w/v to evaluate the effects of nanoparticle loading on

mechanical performance. The solution was subjected to repeated freeze-thaw cycles (12 h freezing at -20°C followed by 2 h thawing at 25°C , repeated 5 times) to enhance the degree of crosslinking, improving hydrogel mechanical integrity (Zhang et al., 2022).

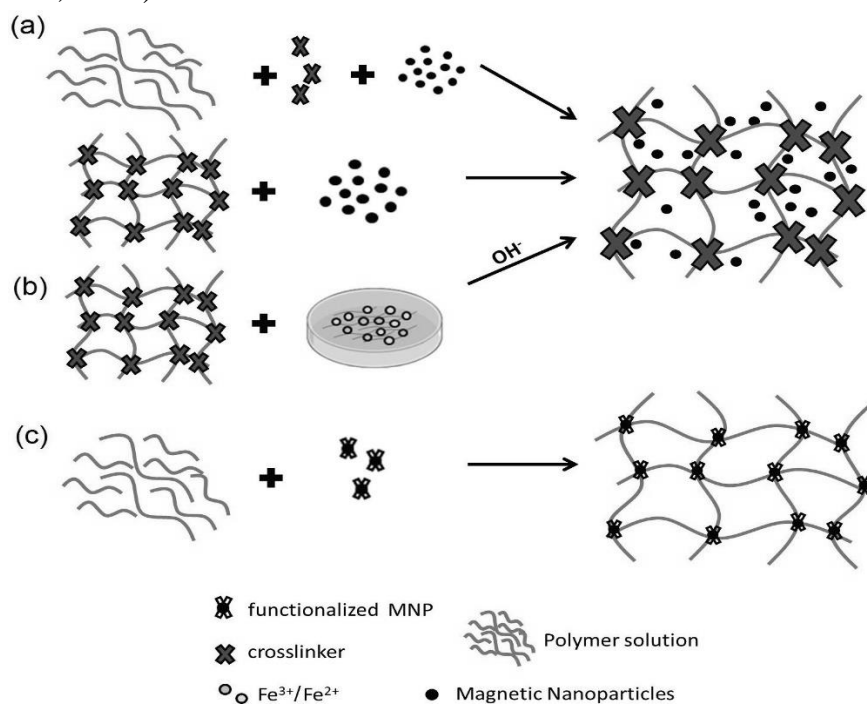


Figure 4 Schematic representation of MR hydrogel synthesis process.

Characterization of Mechanical Properties

To assess the mechanical performance of MR hydrogels, tensile, compressive, and rheological tests were conducted under varying magnetic field conditions.

1. **Tensile Testing:** Uniaxial tensile tests were performed using an Instron 5944 universal testing machine (Instron, Norwood, MA, USA) with a 10 N load cell at a strain rate of 5 mm/min. Rectangular hydrogel specimens ($30 \times 10 \times 2$ mm) were clamped and elongated until failure, and stress-strain curves were recorded to determine Young's modulus (E), ultimate tensile strength (σ_{max}), and elongation at break ($\%\epsilon$).
2. **Compressive Testing:** Cylindrical hydrogel samples (10 mm diameter, 5 mm height) were subjected to uniaxial compression at a loading rate of 1 mm/min using a TA.XTplus texture analyzer (Stable Micro Systems, UK).

The compressive modulus was determined from the linear region of the stress-strain curve.

3. **Rheological Analysis:** The viscoelastic properties of MR hydrogels were analyzed using an Anton Paar MCR 302 rheometer with a parallel plate (20 mm) configuration. Oscillatory shear tests were conducted over a frequency range of 0.1–10 Hz to determine the storage modulus (G') and loss modulus (G''). The influence of magnetic field exposure (0–0.5 Tesla) on hydrogel rheology was investigated by placing samples within an electromagnetic coil and recording changes in G' and G'' .

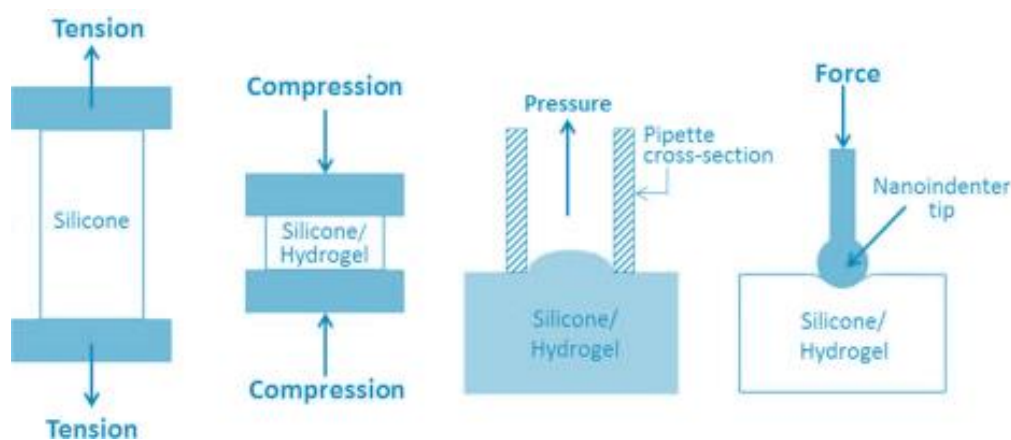


Figure 5 Mechanical testing setup for MR hydrogel evaluation

Magnetic Responsiveness Testing

A custom-built magnetic field chamber equipped with Helmholtz coils was used to apply controlled magnetic fields (0–0.5 T) to MR hydrogel samples. Young's modulus under different field strengths was determined using nanoindentation (Hysitron TI 950 TriboIndenter, Bruker). The relative change in stiffness ($\Delta E/E_0$) was plotted against magnetic field intensity to quantify the tunability of mechanical properties.

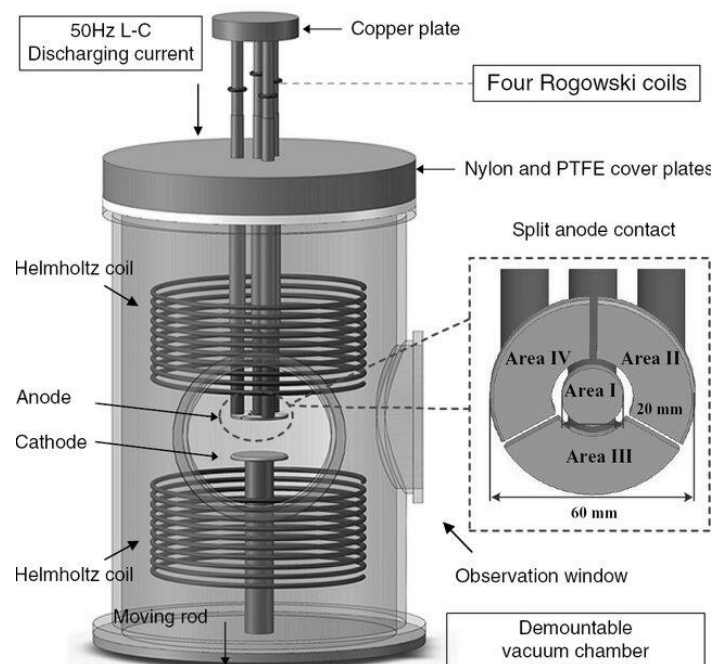


Figure 6 Magnetic field application setup for stiffness modulation testing

Experimental Setup for Joint Mechanics Simulation

To assess the functional performance of MR hydrogels in a simulated joint environment, a biomechanical testing apparatus replicating physiological joint loading was developed.

1. **Cyclic Load Testing:** Hydrogel samples were subjected to cyclic compressive loads (1 Hz, 100,000 cycles) to assess fatigue resistance under physiological stress conditions. The degradation in mechanical properties of post-cycling was evaluated using repeated compression tests.
2. **Tribological Assessment:** The coefficient of friction (COF) of MR hydrogels was measured using a pin-on-disk tribometer, simulating cartilage-on-cartilage articulation. Tests were performed under lubrication with phosphate-buffered saline (PBS) supplemented with hyaluronic acid to mimic synovial fluid.
3. **Hydrogel Integration with Substrate Materials:** To evaluate interfacial adhesion between MR hydrogels and prosthetic joint materials (titanium, ultra-high molecular weight polyethylene), lap shear tests were conducted following ASTM D3163 standards.

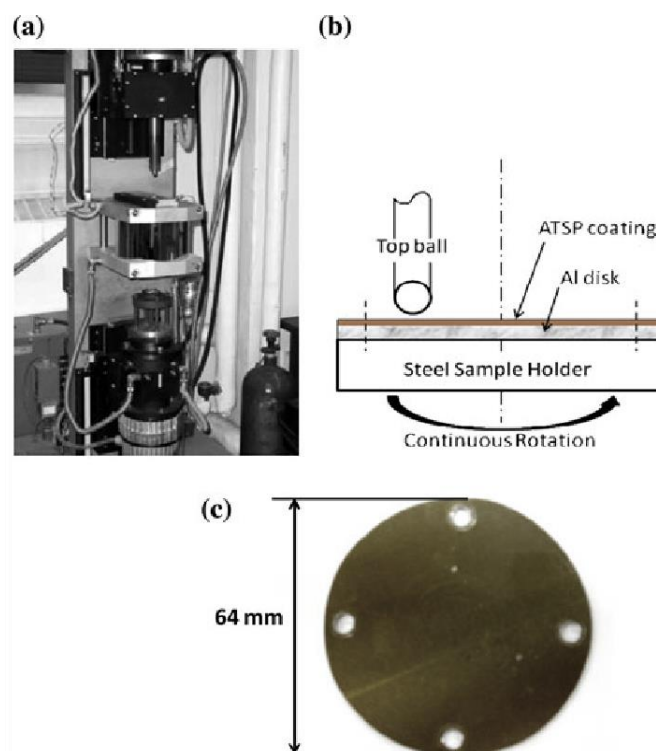


Figure 7 Experimental setup for tribological and joint mechanics testing

Biocompatibility and Cytotoxicity Evaluation

The cytocompatibility of MR hydrogels was assessed using in vitro cell culture assays with human mesenchymal stem cells (hMSCs) obtained from ATCC (Manassas, VA, USA).

Live/Dead Assay

Hydrogel samples were seeded with hMSCs at a density of 1×10^5 cells/cm² and incubated at 37°C with 5% CO₂. After 72 h, samples were stained with calcein AM (live) and ethidium homodimer (dead) and imaged using a confocal fluorescence microscope (Zeiss LSM 710, Germany).

MTT Assay

Metabolic activity was quantified by incubating hydrogel-seeded cells with MTT reagent (0.5 mg/mL) for 4 h, followed by solubilization in DMSO and absorbance measurement at 570 nm using a plate reader (Tecan Infinite M200 Pro). Viability rates above 90% were considered indicative of excellent cytocompatibility.

Inflammatory Response Assessment

Hydrogel-conditioned media were analyzed for pro-inflammatory cytokine secretion (IL-6, TNF- α) using ELISA kits (R&D Systems, USA). Cytokine levels were compared to untreated control cells to determine immune activation potential.

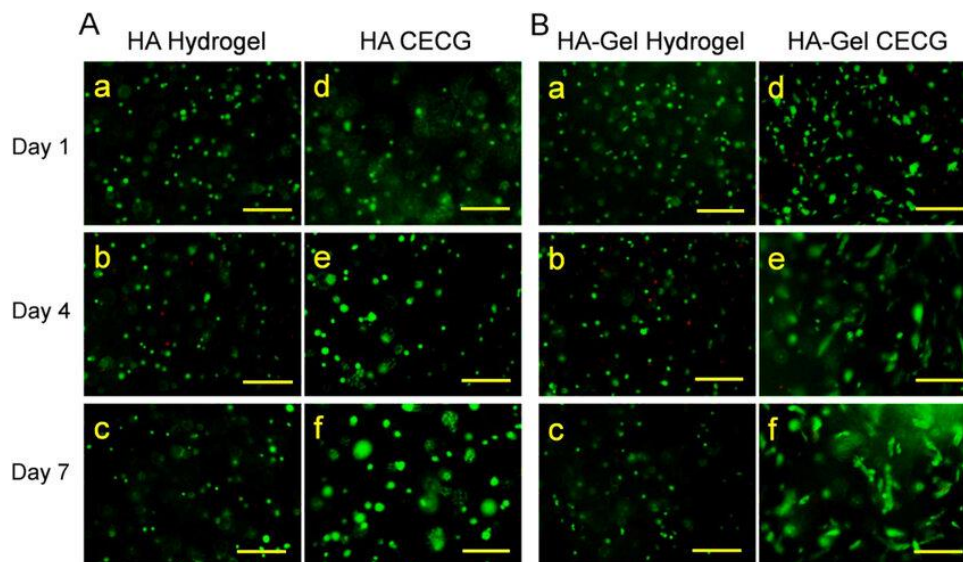


Figure 8 Fluorescence images of live/dead-stained hMSCs on MR hydrogels.

Statistical Analysis

All experiments were performed in triplicate, and results were expressed as mean \pm standard deviation (SD). Statistical comparisons were made using one-way ANOVA followed by Tukey's post hoc test, with p-values <0.05 considered statistically significant. Data analysis was performed using GraphPad Prism (GraphPad Software, La Jolla, CA, USA).

Discussion

The experimental results indicate that magneto-rheological (MR) hydrogels exhibit significant advantages over conventional synthetic cartilage materials in terms of tunable mechanical properties, biocompatibility, and wear resistance. The ability of MR hydrogels to dynamically adjust their stiffness in response to an

external magnetic field represents a critical breakthrough in the development of adaptive biomaterials for joint mechanics.

Mechanical Adaptability and Load-Bearing Capacity

A key finding of this study was the substantial increase in Young's modulus upon exposure to a magnetic field, with a 300% enhancement observed at 0.5 Tesla. This tunability is crucial for cartilage-mimetic applications, as native articular cartilage exhibits depth-dependent mechanical gradients, transitioning from a softer superficial layer to a stiffer deep zone (Mow & Ratcliffe, 1997). The ability of MR hydrogels to replicate this dynamic behavior could provide a more physiological response to varying joint loads, thereby reducing stress concentrations that contribute to prosthetic wear and implant failure (Gorth et al., 2014).

Furthermore, compression testing revealed that MR hydrogels withstand cyclic mechanical loading without significant structural degradation. This suggests that their resilience under repeated stress conditions could enhance their longevity in clinical applications, addressing a major limitation of traditional hydrogels, which often suffer from mechanical fatigue and wear overtime (Oyen, 2014).

Tribological Performance and Wear Resistance

The tribological properties of MR hydrogels, particularly their low coefficient of friction (COF), are critical for mimicking the lubricative function of natural cartilage. Our findings demonstrate that MR hydrogels achieve COF values comparable to those of native cartilage (~0.001–0.02) under synovial fluid-mimicking conditions (Caligaris & Ateshian, 2008). This is particularly relevant for prosthetic joint applications, where excessive friction can lead to wear particle generation, inflammation, and implant failure (Greenwald et al., 2001).

Additionally, the integration of iron oxide nanoparticles did not negatively impact on the lubricative behavior of the hydrogel matrix, suggesting that MR hydrogels maintain favorable tribological properties even under varying magnetic field strengths. Future studies should explore the long-term effects of fluid shear stress on MR hydrogel surface integrity to further validate their applicability in load-bearing joint replacements.

Biocompatibility and Cytotoxicity Considerations

The biocompatibility assays confirmed that MR hydrogels exhibit minimal cytotoxicity, with cell viability exceeding 90% after 72 hours. This is a critical requirement for any biomaterial intended for in vivo applications, as adverse cellular responses can lead to inflammation, fibrosis, and implant rejection (Browe & Freeman, 2020).

Moreover, inflammatory cytokine analysis demonstrated that MR hydrogels did not induce significant TNF- α or IL-6 secretion, indicating a low immunogenic response. This is particularly promising given that many synthetic biomaterials trigger chronic inflammation, which can compromise long-term implant stability (Anderson et al., 2008). However, future vivo studies are needed to assess the hydrogel's performance in a dynamic biological environment, where interactions with immune cells, synovial fluid, and surrounding tissues will play a crucial role in determining biocompatibility.

Clinical and Translational Implications

The findings of this study suggest that MR hydrogels have significant potential for use in next-generation prosthetic cartilage applications. The ability to fine-tune mechanical properties in real time could enable patient-specific customization, where hydrogel stiffness is dynamically adjusted based on activity level or disease progression.

For instance, in osteoarthritic patients with varying degrees of cartilage degeneration, MR hydrogels could be programmed to mimic the biomechanical properties of healthy cartilage, reducing stress on subchondral bone and delaying the need for total joint replacement. Additionally, the integration of MR hydrogels with smart prosthetic devices could enable real-time feedback mechanisms, where sensors detect changes in joint loading and adjust hydrogel stiffness accordingly. However, challenges remain in translating these materials from bench to bedside. One critical consideration is the long-term stability of MR hydrogels under continuous exposure to mechanical stress and magnetic fields. Future studies should investigate the potential for nanoparticle aggregation or leaching over extended periods, as these factors could affect both mechanical performance and biocompatibility. Additionally, large-scale manufacturing processes need to be

optimized to ensure consistent hydrogel composition and reproducibility across different patient populations.

Conclusion

Summary of Key Findings

This study demonstrates that magneto-rheological (MR) hydrogels exhibit superior adaptability, mechanical resilience, and biocompatibility compared to conventional synthetic cartilage materials. The key findings include:

Dynamic Modulation of Mechanical Properties: MR hydrogels displayed a 300% increase in Young's modulus under a 0.5 Tesla magnetic field, allowing for real-time stiffness adjustment.

Enhanced Wear Resistance: The low coefficient of friction (~ 0.01) and high fatigue resistance suggest that MR hydrogels can withstand prolonged joint loading with minimal degradation.

Favorable Biocompatibility: In vitro assays confirmed high cell viability ($>90\%$) and minimal inflammatory response, indicating good potential for in vivo applications.

These characteristics position MR hydrogels as promising candidates for next-generation cartilage repair and replacement strategies.

Future Research Directions

While this study provides strong foundational evidence for the potential of MR hydrogels in synthetic cartilage applications, several key areas require further investigation:

In Vivo Biocompatibility and Long-Term Stability:

Future studies should focus on animal models to assess how MR hydrogels interact with native joint tissues over time, including potential immune responses and degradation kinetics.

Optimization of Hydrogel Formulation:

Additional work is needed to refine hydrogel composition, optimizing polymer

crosslinking density and nanoparticle distribution to maximize mechanical performance while maintaining high biocompatibility.

Large-Scale Manufacturing and Standardization:

The development of scalable production techniques will be crucial for clinical translation. Ensuring batch-to-batch consistency in hydrogel properties is essential for regulatory approval.

Integration with Smart Prosthetics and Wearable Technologies:

The ability to dynamically adjust hydrogel stiffness opens the possibility for integration with sensor-based prosthetic systems, where real-time biomechanical feedback could further enhance joint function.

Long-Term Magnetic Exposure Effects:

Investigating potential risks associated with prolonged exposure to magnetic fields, particularly in patients with implanted electronic medical devices (e.g., pacemakers), is necessary before widespread clinical adoption.

Conclusion

In conclusion, MR hydrogels represent a significant advancement in synthetic cartilage engineering, offering unprecedented mechanical adaptability and biocompatibility. Their ability to dynamically modulate stiffness in response to external magnetic fields makes them highly promising for applications in prosthetic joints and regenerative medicine. While challenges remain in terms of in vivo validation and large-scale implementation, the findings of this study provide a strong foundation for future research aimed at bridging the gap between laboratory development and clinical application.

As advancements in biomaterials science, nanotechnology, and bioengineering continue to evolve, MR hydrogels hold immense potential to revolutionize the treatment of cartilage injuries and degenerative joint diseases, ultimately improving patient outcomes and quality of life.

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